Link between Tomography and Copula

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Abstract

An important problem in statistics is to determine a joint probability distribution from its marginals and an important problem in Computed Tomography (CT) is to reconstruct an image from its projections. In the bivariate case, the marginal probability density functions $f_1(x)$ and $f_2(y)$ are related to their joint distribution $f(x, y)$ via horizontal and vertical line integrals. Interestingly, this is also the case of a very limited angle X ray CT problem where $f(x, y)$ is an image representing the distribution of the material density and $f_1(x)$, $f_2(y)$ are the horizontal and vertical line integrals. The problem of determining $f(x, y)$ from $f_1(x)$ and $f_2(y)$ is an ill-posed undetermined inverse problem. In statistics the notion of *copula* is exactly introduced to characterize all the possible solutions to the problem of reconstructing a bivariate density from its marginals. In this paper, we elaborate on the possible link between Copula and CT and try to see whether we can use the methods used in one domain into the other.

Key words: Copula, Tomography, Joint and marginal distributions, Image reconstruction, Additive and Multiplicative Backprojection, Maximum

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Entropy, Archimedean Copulas.

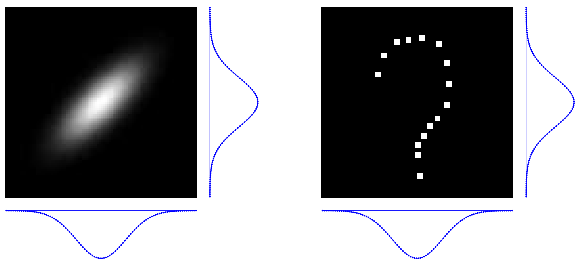
1. Introduction

The word *copula* originates from the Latin meaning *link, chain, union.* In statistical literature, according to the seminal result in the copula's theory stated by Abe Sklar [1] in 1959, a copula is a function that connects a multivariate distribution function to its univariate marginal distributions. There is an increasing interest concerning copulas, widely used in Financial Mathematics and in modelling of Environmental Data [2, 3]. Recently, in Computational Biology, copulas were used for the reconstruction of accurate cellular networks [4]. Copula appear to be a powerful tool to model the structure of dependence [5, 6]. Copulas are useful for constructing joint distributions, particularly with non-Gaussian random variables [7].

In 2D case, interpreting the joint probability density function $f(x, y)$ as an image and its marginal probability densities $f_1(x)$ and $f_2(y)$ as horizontal and vertical line integrals:

$$f_1(x) = \int f(x, y)\ \mathrm{d}y \quad \text{and} \quad f_2(y) = \int f(x, y)\ \mathrm{d}x \tag{1}$$

we see that the problem of determining $f(x, y)$ from $f_1(x)$ and $f_2(y)$ is an ill-posed (inverse) problem [8]. It is a well known fact that while a distribution has a unique set of marginals, the converse is not necessarily true. That is, many distributions may share a common subset of marginals. In general, it is not possible to uniquely reconstruct a distribution from its marginals.



Forward problem: Given $f(x,y)$ compute $f_1(x)$ and $f_2(y)$

(a)

Inverse problem: Given $f_1(x)$ and $f_2(y)$ determine $f(x,y)$

(b)

Figure 1: Forward and inverse problems

This is illustrated in Figure 1: Fig.1 (a) shows the forward problem given by (1), whereas Fig.1 (b) illustrates the inverse problem. As we will see later, all functions in the form of

$$f(x,y) = f_1(x)\, f_2(y)\, \Omega(x,y) \tag{2}$$

where $\Omega(x,y) = c(F_1(x), F_2(y))$ and $c(u,v)$ is any *copula* density function, are solutions of this problem. Interestingly, this is very similar to the pdf reconstruction problem considered in [9], where a special *copula* was designed. The approach in [9] could certainly be interpreted using the results presented here.

In 1917, Johann Radon introduced the Radon transform (RT) [10, 11] which was later used in CT [12]. Indeed, if we denote by $f(x,y)$, the spatial distribution of the material density in a section of the body, a very simple model that relates a line of the radiography image $p(r,\theta)$ at direction θ to $f(x,y)$ is given by the Radon transform:

$$p(r,\theta) = \int_{L_{r,\theta}} f(x,y)\ \mathrm{d}l = \iint_{\mathcal{R}^2} f(x,y)\delta(r - x\cos\theta - y\sin\theta)\ \mathrm{d}x\ \mathrm{d}y. \quad (3)$$

The experimental setup is presented in Figure 3.

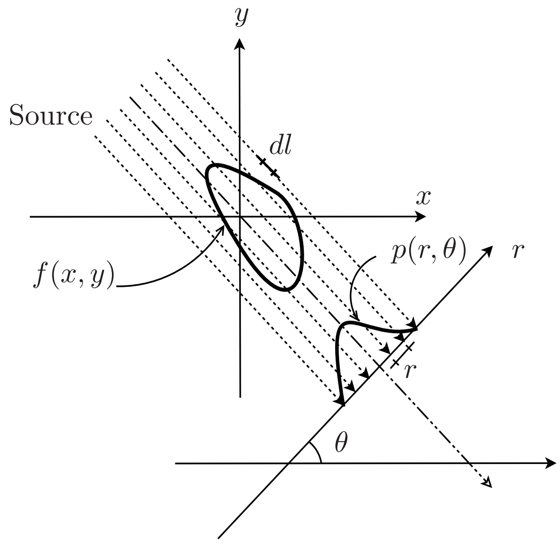


Figure 2: X ray Computed Tomography: 2D parallel geometry.

If now we consider only the horizontal $\theta = 0$ projection and the vertical $\theta = \pi/2$ projection, we see easily the connexion between these two problems. The main object of this paper is to explore in more details these relations, and exploit the similarity between the two problems as a new approach to image reconstruction in Computed Tomography.

The rest of this paper is organized as follows: In section 2, we present a summary of the necessary definitions and properties of copulas and highlight methods to generate a copula. In section 3, we present the main tomographic image reconstruction methods based on the Radon inversion formula. In section 4, we will be in the heart of the link and relations between the notions of these two previous sections. Section 5 and 6 are devoted to details concerning our method. Some preliminary results from our Copula-Tomography Matlab package [13] which available for download are given in section 6.

2. Copula

In this section, we give a few definitions and properties of copulas that we need in the rest of the paper. First, we note by $F(x,y)$ a bivariate cumulative distribution function (cdf), by $f(x,y)$ its bivariate probability density function (pdf), by $F_1(x)$, $F_2(y)$ its marginal cdf's and $f_1(x)$, $f_2(y)$ their corresponding pdf's with their classical relations:

$$\begin{aligned}
F(x,y) &= \int_{-\infty}^{x}\int_{-\infty}^{y} f(u,v)\ \mathrm{d}u\ \mathrm{d}v, \quad f(x,y) = \frac{\partial^2 F(x,y)}{\partial x\,\partial y}, \\
F_1(x) &= \int_{-\infty}^{x} f_1(u)\ \mathrm{d}u = F(x,\infty), \quad F_2(y) = \int_{-\infty}^{y} f_2(v)\ \mathrm{d}v = F(\infty,y), \\
f_1(x) &= \frac{\mathrm{d}F_1(x)}{\mathrm{d}x} = \int f(x,y)\ \mathrm{d}y, \quad f_2(y) = \frac{\mathrm{d}F_2(y)}{\mathrm{d}y} = \int f(x,y)\ \mathrm{d}x.
\end{aligned}$$

Definition 1. *Bivariate Copula: A bivariate copula, or shortly a copula is a function from* $[0,1]^2$ *to* $[0,1]$ *with the following properties:*

- $\forall u,v \in [0,1]\,,\quad C(u,0) = 0 = C(0,v)$*;*
- $\forall u,v \in [0,1]\,,\quad C(u,1) = u$ *and* $C(1,v) = v$*;*
- $\forall u_1,u_2,v_1,v_2 \in [0,1]$ *such that* $u_1 \leq u_2$ *and* $v_1 \leq v_2$, $C(u_2,v_2) - C(u_2,v_1) - C(u_1,v_2) + C(u_1,v_1) \geq 0.$

Theorem 1. *Sklar's Theorem: Let F be a two-dimensional distribution function with marginal distributions functions F_1 and F_2. Then there* ***exists*** *a copula C such that:*

$$F(u, v) = C(F_1(x), F_2(y)). \tag{4}$$

Conversely, *for any univariate distribution functions F_1 and F_2 and any copula C, the function F is a two-dimensional distribution function with marginals F_1 and F_2, given by (4). Furthermore, if the marginal functions are continuous, then the copula C is* ***unique***, *and is given by*

$$C(u, v) = F(F_1^{-1}(u), F_2^{-1}(v)). \tag{5}$$

Definition 2. *Copula Density: From (4) and differentiating (5) gives the density of a copula*

$$c(u, v) = \frac{\partial^2 C}{\partial u \, \partial v} = \frac{f\left(F_1^{-1}(u), F_2^{-1}(v)\right)}{f_1\left(F_1^{-1}(u)\right) \, f_2\left(F_2^{-1}(v)\right)}, \tag{6}$$

and thus

$$f(x, y) = f_1(x) \, f_2(y) \, c(F_1(x), F_2(y)) \tag{7}$$

An usual simple example is the **product** or **independent** copula:

$$C(u, v) = u \, v \longrightarrow c(x, y) = 1, \quad (u, v) \in [0, 1]^2 . \tag{8}$$

Property 1. *Any copula $C(u, v)$, satisfies the inequality*

$$W(u, v) \leq C(u, v) \leq M(u, v), \tag{9}$$

where the ***Fréchet-Hoeffding upper bound copula*** *$M(u, v)$ (or comonotonicity copula) is :*

$$M(u, v) = \min(u, v), \quad (u, v) \in [0, 1]^2 . \tag{10}$$

*and the **Fréchet-Hoeffding lower bound** $W(u,v)$ (or countermonotonicity copula) is:*

$$W(u,v) = \max\{u+v-1, 0\}, \quad (u,v) \in [0,1]^2. \tag{11}$$

Generating Copulas by the Inversion Method: A straight forward method is based directly on Sklar's theorem. Given $F(x,y)$ the joint cdf of two variables X, Y and $F_1(x)$ and $F_2(y)$ their marginal cdf's, all assumed to be continuous. The corresponding copula can be constructed by using the unique inverse transformations (Quantile transform) $x = F_1^{-1}(u)$, $y = F_2^{-1}(v)$,

$$C(u,v) = F(F_1^{-1}(u), F_2^{-1}(v)), \tag{12}$$

where u, v are uniform on $[0,1]$.

Archimedean Copulas: The Archimedean copulas form an important class of copulas ([14] page 109) which generalise the usual copulas.

Theorem 2. *Let φ be a continuous, strictly decreasing function from $[0,1]$ to $[0,\infty]$ such that $\varphi(1) = 0$, and let $\varphi^{[-1]}$ be the pseudo-inverse of φ. Let C be the function from $[0,1]^2$ to $[0,1]$ given by*

$$C(u,v) = \varphi^{[-1]}(\varphi(u) + \varphi(v)). \tag{13}$$

Then C is a copula if and only if φ is convex.

Archimedean copulas are in the form (13) and the function φ is called the generator of the copula. φ is a strict generator if $\varphi(0) = \infty$, then $\varphi^{[-1]} = \varphi^{-1}$ and

$$C(u,v) = \varphi^{-1}(\varphi(u) + \varphi(v)). \tag{14}$$

Property 2. *The following algebraic properties are satisfied by any Archimedean copula C:*

- $C(u, v) = C(v, u)$ *meaning that C is symmetric;*
- $C(C(u, v), w) = C(u, C(v, w))$;
- *If $a > 0$, then $a\varphi$ is again a generator of C.*

Theorem 3. *Let C be an Archimedean copula with generator φ in Ω. Then for almost all u and v in $[0, 1]$,*

$$\varphi^{'}(u)\frac{\partial C(u,v)}{\partial v} = \varphi^{'}(v)\frac{\partial C(u,v)}{\partial u}. \tag{15}$$

Property 3. *One easy way to compute the bivariate copula density function $c(u,v)$ of the copula $C(u,v)$, using the generator function φ under some conditions is given by:*

$$c(u,v) = -\frac{\varphi^{''}(C(u,v))\varphi^{'}(u)\varphi^{'}(v)}{[\varphi^{'}(C(u,v))]^3}. \tag{16}$$

3. Tomography

In 2D, the mathematical problem of tomography is to determine the bivariate function $f(x,y)$ from its line integrals $p(\theta, r)$ (see Eq.(3)). Radon has shown that this problem has a unique solution if we know $p(r,\theta)$ for all $\theta \in [0,\pi]$ and all $r \in \mathcal{R}$ and can be computed by so called the inverse Radon transform

$$f(x,y) = \frac{1}{2\pi}\int_0^{\pi}\int_0^{\infty}\frac{\frac{\partial p(r,\theta)}{\partial r}}{r - x\cos\phi - y\sin\phi}\,\mathrm{d}r\,\mathrm{d}\phi \tag{17}$$

However, if the number of projections is limited, then the problem is ill-posed and the problem has an infinite number of solutions.

To present briefly the main classical methods in CT, we start by decomposing the inverse RT in the following parts:

$$\text{Derivative } \mathcal{D}: \quad \overline{p}_\theta(r) = \frac{\partial p(r,\theta)}{\partial r},$$

$$\text{Hilbert Transform } \mathcal{H}: \quad \widetilde{\overline{p}}(r',\theta) = \frac{1}{\pi}\int_0^\infty \frac{\overline{p}(r,\theta)}{(r-r')}\,\mathrm{d}r,$$

$$\text{Backprojection } \mathcal{B}\text{: } f(x,y) = \frac{1}{2\pi}\int_0^\pi \widetilde{\overline{p}}(x\cos\theta + y\sin\theta, \theta)\,\mathrm{d}\theta.$$

Then defining the one dimensional inverse Fourier transform $\mathcal{F}_1^{-1}$ by

$$P(\Omega,\theta) = \int p(r,\theta)\,\exp\left[j\Omega r\right]\,\mathrm{d}r$$

and using the properties of the Fourier transform $\mathcal{F}_1$ and the derivative $\mathcal{D}$:

$$\bar{P}(\Omega,\theta) = \Omega P(\Omega,\theta),$$

the relation between $\mathcal{H}$ and $\mathcal{F}_1$ yields :

$$\widetilde{\bar{P}}(\Omega,\theta) = \operatorname{sign}(\Omega)\Omega\bar{P}(\Omega,\theta) = |\Omega| P(\Omega,\theta).$$

Finally the *filtered backprojection* which is currently the most used reconstruction method is performed by the following formula :

$$f(x,y) = \mathcal{B}\,\mathcal{H}\,\mathcal{D}\,p(r,\theta) = \mathcal{B}\,\mathcal{F}_1^{-1}\,|\Omega|\,\mathcal{F}_1\,p(r,\theta) \tag{18}$$

that is

$$\xrightarrow{p(r,\theta)} \boxed{\begin{matrix}\text{FT}\\ \mathcal{F}_1\end{matrix}} \longrightarrow \boxed{\begin{matrix}\text{Filter}\\ |\Omega|\end{matrix}} \longrightarrow \boxed{\begin{matrix}\text{IFT}\\ \mathcal{F}_1^{-1}\end{matrix}} \longrightarrow \boxed{\begin{matrix}\text{Backprojection}\\ \mathcal{B}\end{matrix}} \xrightarrow{f(x,y)}$$

In X-ray CT, if we have a great number of projections uniformly distributed over the angles interval $[0, \pi]$, the filtered backprojection (FBP) or even the simple backprojection (BP) image are good solutions to the inverse CT problem [15]. But, when we are restricted to only two projections, the FBP or BP images are not correct reconstruction [16–18].

4. Link between Copula and Tomography

Now, let consider the particular case where we have only two projections $\theta = 0$ and $\theta = \pi/2$. Then

$$\begin{aligned} p_0(r) &= \iint f(x,y)\delta(r-x)\, \mathrm{d}x\, \mathrm{d}y = \int f(r,y)\, \mathrm{d}y, \\ p_{\pi/2}(r) &= \iint f(x,y)\delta(r-y)\, \mathrm{d}x\, \mathrm{d}y = \int f(x,r)\, \mathrm{d}x \end{aligned}$$

and if we let $f_1 = p_0$ and $f_2 = p_{\pi/2}$ we can deduce the following new methods, inspired by the reconstruction approaches in CT, for the inverse problem that consists in determining the probability density $f(x,y)$ from its marginals $f_1(x)$ and $f_2(y)$:

Backprojection:

$$f(x,y) = \frac{1}{2}(f_1(x) + f_2(y)). \tag{19}$$

Filtered Backprojection:

$$f(x,y) = \frac{1}{2}\left(\int \frac{\frac{\partial f_1}{\partial x}(x')}{x'-x}\, \mathrm{d}x' + \int \frac{\frac{\partial f_2}{\partial y}(y')}{y'-y}\, \mathrm{d}y'\right) \tag{20}$$

which can also be implemented in the Fourier domain as it follows

$$\begin{aligned} f(x,y) &= \tfrac{1}{2}\int e^{+jux}|u| \left(\int e^{-jux'} f_1(x')\, \mathrm{d}x'\right)\, \mathrm{d}u \\ &+\tfrac{1}{2}\int e^{+jvy}|v| \left(\int e^{-jvy'} f_2(y')\, \mathrm{d}y'\right)\, \mathrm{d}v. \end{aligned}$$

5. How to use Copula in Tomography

The definition and the notion of copula give us the possibility to propose new X ray CT methods. Let first consider the case of two projections. In this case, immediately, we can propose a first use which corresponds to the case of independent copula, as given in (8). We call this method *Multiplicative Backprojection (MBP)*, [19]

MBP:

$$f(x,y) = f_1(x)\, f_2(y) \tag{21}$$

If we compare the equation (19) to (21) instead of the classical BP which is an additive operation or *Additive Backprojection*, the name MBP comes naturally. In Figure 3 we give comparisons of BP and MBP. As we can see on the image original 1, at least the image obtained by MBP is better than the one obtained by BP and it satisfies exactly the marginals.

We may still do better if we used choose another copula rather than the independent copula, by proposing the following method that we call *Copula Backprojection (CopBP).*

CopBP:

$$f(x,y) = f_1(x)\, f_2(y)\, c\,(F_1(x), F_2(y)) \tag{22}$$

where $c(u,v)$ is a parametrized copula.

Here the main question is how to choose an appropriate copula for the particular application. This problem can be thought as a way to introduce some prior information, just enough to choose an appropriate family of copula. For example if we know that the joint density has only one mode, and can be approximated by a bivariate Gaussian, Φ^{-1} denoting the inverse of the standard Gaussian cdf, then we can use a Gaussian copula whose expression is given by

$$C_\rho(u,v) = \frac{A}{2\pi} \int_{-\infty}^{\Phi^{-1}(u)} \int_{-\infty}^{\Phi^{-1}(v)} \exp\left\{ \frac{-(s^2 - 2\rho st + t^2)}{2(1-\rho^2)} \right\} ds\, dt$$

where $A = \left(1-\rho^2\right)^{-1/2}$ and the particular cases where $\rho = -1, 0, 1$ correspond respectively to copulas $W(u,v)$, $\Pi(u,v)$ and $M(u,v)$. The corresponding Gaussian copula density is :

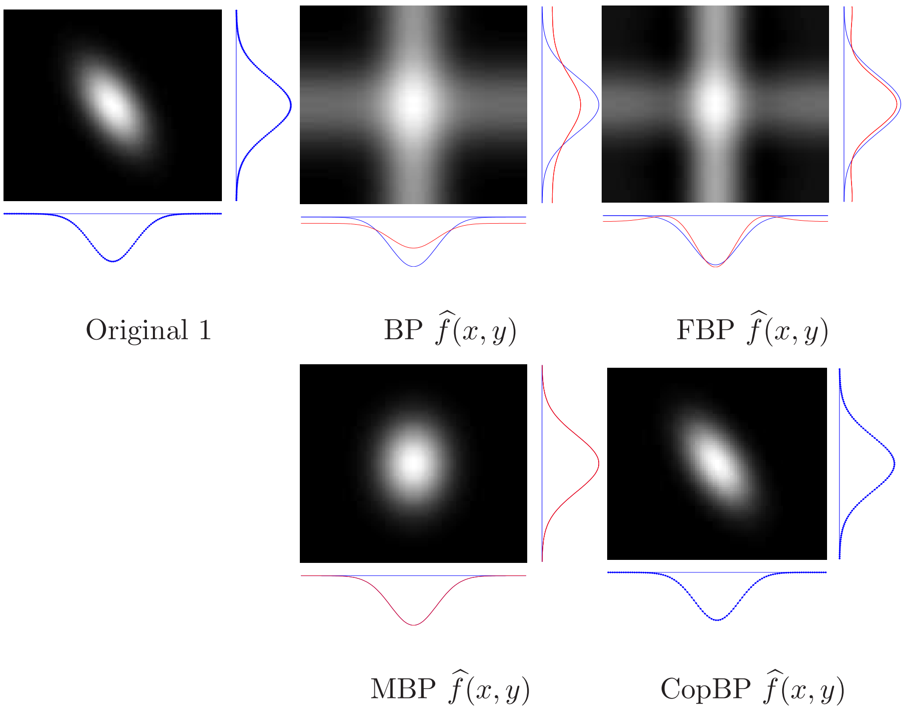
$$c_\rho(u,v) = A \exp\left\{ \frac{-A^2}{2} \left((\rho u)^2 - 2\rho uv + (\rho v)^2\right) \right\}.$$

Finally, the function $f(x,y)$ we are looking for will be :

$$f(x,y) = A f_1(x) f_2(y) \exp\left\{ -\frac{\left(\rho^2 x^2 - 2\rho xy + \rho^2 y^2\right)}{2(1-\rho^2)} \right\} \tag{23}$$

where $\Phi^{-1}(u) = x$ and $\Phi^{-1}(v) = y$. The particular reconstruction (23) is parametrized the correlation coefficient ρ, which, of course, shall be estimated. Figure 3 presents CopBP reconstructions obtained using this Gaussian copula. We see the interest of such an approach compared to standard BP, although, of course, it should be refined, by incorporation of more prior knowledge.

Example 1 :



Example 2 :

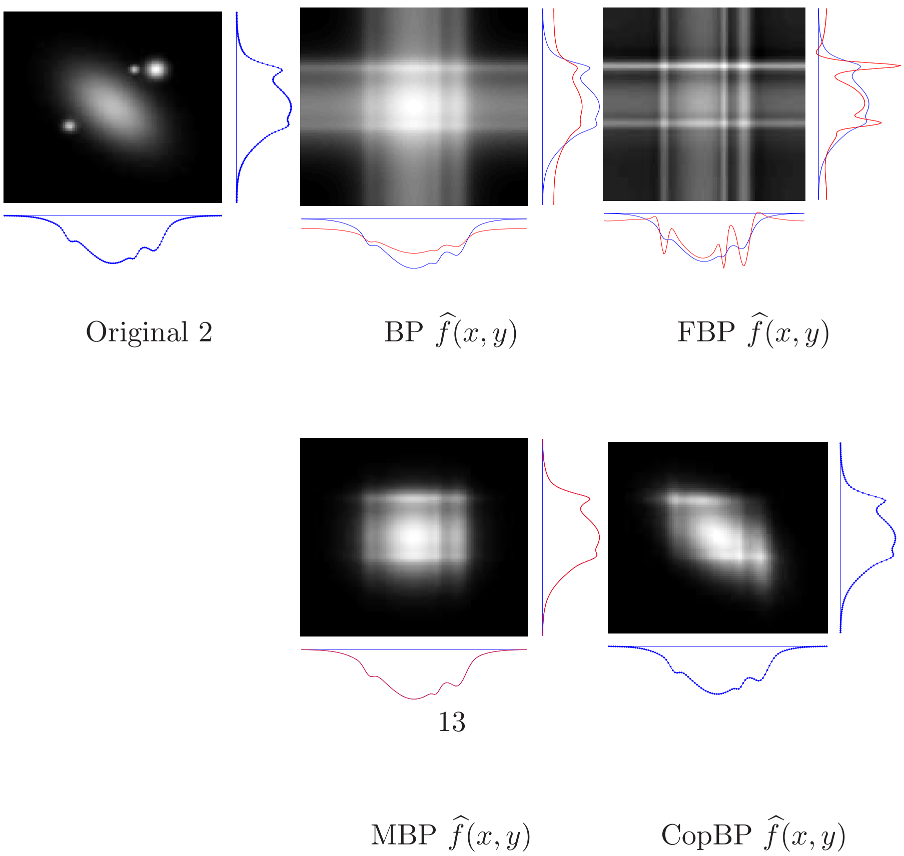


Figure 3: A comparison between BP, FBP, MBP and CopBP on two synthetic examples.

6. Maximum Entropy Copulas

The selection of a particular copula is a difficult task. We propose here to look at this ill-posed inverse problem by so called maximum entropy (ME) method, using copula. The principle of ME was first expounded by E.T. Jaynes in two seminal papers in 1957 ([20, 21]). It is the way to assign a probability distribution to a quantity on which we have partial information. The classical ME problem is to assign a probability law to a quantity on which we only know a few moments. Here, the problem is a bit different, because the partial information we have is not in terms of moments but in the form of the following constraints:

$$\begin{cases} C_1 : \displaystyle\int f(x,y)\,dy = f_1(x), & \forall y \\ C_2 : \displaystyle\int f(x,y)\,dx = f_2(y), & \forall x \\ C_3 : \displaystyle\iint f(x,y)\,dx\,dy = 1. & \end{cases} \tag{24}$$

Hence, the goal is to find the most general copula, in the ME sense, compatible with available information, that is, with the marginals/projections at hands.

6.1. Problem's formulation

Among all possible $f(x,y)$ satisfying the constraints (24) choose the one which optimizes a criterion $\Omega(f)$, i.e :

$$\hat{f} := \text{maximize } \{\Omega(f)\} \textit{ subject to } (24).$$

Since the constraints are linear, if we choose a criterion which is a concave function, then there is a unique solution to the problem. Many entropies functional can serve as an objective function, e.g. [22–27] :

1. $\Omega_1(f) = -\iint |\, f(x,y) \,|^2 \; dx\, dy, \quad (-\text{Energy or } \mathrm{L}_2 - \text{ norm})$
2. $\Omega_2(f) = -\iint f(x,y) \ln f(x,y)\, dx\, dy, \quad (\text{Shannon Entropy}),$
3. $\Omega_3(f) = \iint \ln f(x,y)\, dx\, dy, \quad (\text{Burg Entropy}),$
4. $\Omega_4(f) = \frac{1}{1-\alpha} \iint (f^\alpha(x,y) - 1)\; dx\, dy, \quad (\text{Tsallis Entropy})$
5. $\Omega_5(f) = \frac{1}{1-\alpha} \ln \iint f^\alpha(x,y)\, dx\, dy, \quad (\text{Rényi Entropy}).$

Our main contribution here is to find the generic expression for the solution of these criteria. The main tool is the classical Lagrange multipliers technique which consists in defining the Lagrangian functional

$$\begin{aligned}\mathcal{L}_g(f, \lambda_0, \lambda_1, \lambda_2) = \Omega(f) &+ \lambda_0 \left(1 - \iint f(x,y) dx dy\right) \\ &+ \int \lambda_1(x) \left(f_1(x) - \int f(x,y) dy\right) dx \\ &+ \int \lambda_2(y) \left(f_2(y) - \int f(x,y) dx\right) dy,\end{aligned}$$

and find its stationnary point which is defined as the solution of the following system of equations:

$$\begin{cases} \dfrac{\partial \mathcal{L}_g(f, \lambda_0, \lambda_1, \lambda_2)}{\partial f} = 0, \\ \dfrac{\partial \mathcal{L}_g(f, \lambda_0, \lambda_1, \lambda_2)}{\partial \lambda_i} = 0. \end{cases}$$

Here, we do not show all the details, but only give the final expression, assuming that the integrals converge:

1. $\hat{f}(x,y) = -\frac{1}{2}\left(\lambda_1(x) + \lambda_2(y) + \lambda_0\right)$, (-Energy)

2. $\hat{f}(x,y) = \exp(-\lambda_1(x) - \lambda_2(y) - \lambda_0)$, (Shannon entropy)

3. $\hat{f}(x,y) = \dfrac{1}{\lambda_1(x) + \lambda_2(y) + \lambda_0}$, (Burg entropy)

4. $\hat{f}(x,y) = \dfrac{1-\alpha}{\alpha}\left(\lambda_1(x) + \lambda_2(y) + \lambda_0\right)^{\frac{1}{\alpha-1}}$, (Tsallis and Renyi entropies).

Where $\lambda_1(x)$, $\lambda_2(y)$ and λ_0 are obtained by replacing these expressions in the constraints (24) and solving the resulting system of equations. When solving the Lagrangian functional equation which is concave in f, we assume that there exists a feasible $f > 0$ with finite entropy. The results for Tsallis and Renyi entropies leads to the same family of distribution depending on α due to the monotonicity property of the logarithm function. For the two criteria -Energy and Shannon entropy, we can find analytical solutions for $\lambda_1(x)$, $\lambda_2(y)$ and λ_0. For $-Energy$, we obtain:

$$\lambda_1(x) = -2f_1(x) + \int \lambda_1(x)\ \mathrm{d}x + 2,\ \lambda_2(y) = -2f_2(y) + \int \lambda_2(y)\ \mathrm{d}y + 2$$

and $\lambda_0 = -2 - \int \lambda_1(x)\ \mathrm{d}x - \int \lambda_2(y)\ \mathrm{d}y$, which finally gives:

$$\hat{f}(x,y) = f_1(x) + f_2(y) - 1. \tag{25}$$

This is nothing else but the standard Back Projection mechanism (up to scale factor and a constant). Hence, the Back projection method can be easily interpreted as a minimum norm solution. For the Shannon entropy, we get:

$$\lambda_1(x) = -\ln\left(f_1(x)\int \lambda_1(x)\ \mathrm{d}x\right),$$

$$\lambda_2(y) = -\ln\left(f_2(y)\int \lambda_2(y)\ \mathrm{d}y\right) \text{ and}$$

$\lambda_0 = \ln\left(\int \lambda_1(x)\ \mathrm{d}x \int \lambda_2(y)\ \mathrm{d}y\right)$ which yields

$$\hat{f}(x, y) = f_1(x) f_2(y). \tag{26}$$

This is now the MBP we obtained as associate to an independent copula. Unfortunately, in the the cases of Burg, Tsallis and Renyi entropies, it is not possible to find analytical expressions for λ_0, λ_1, and λ_2 as functions of f_1 and f_2. Consequently a numerical approach is required, see for example [28].

Using equation (22) one can write all entropies in terms of copulas. For example, if we denote the Shannon entropy by $H(x, y)$ and the copula entropy by $H_c(u, v)$, then :

$$H(x, y) = H(x) + H(y) + H_c(u, v).$$

The previous relation shows that the Shannon entropy of the bivariate distribution is the sum of the entropies provided by each marginal density and the copula entropy. And the extension in the multivariate case is straightforward. Therefore, maximizing the joint entropy, given the marginals, is equivalent to maximize the entropy of the copula $H_c(u, v)$. Since we only have here a domain constraint -the copula is defined on $[0, 1]^2$-, the Shannon Maximum entropy copula is uniform, $c(u, v) = 1$, and we obtain the MBP reconstruction (26). Now, if we look for a Shannon maximum entropy copula with an additional correlation constraint-that is we fix the correlation of the underlying normalized random variables-,then we end with a Gaussian copula, which in turn, lead us to the CopBP method with a Gaussian copula (22). Along these lines, it seems possible to characterize the different families of copula as maximum entropy solutions, possibly incorporating more prior information. More generally, it will also be interesting to characterize the copulas corresponding to the Burg/Rényi ME solutions.

Some simulations are reported Figure 3. The aim of these simulations from our copula-tomography package [13] is just to show the link between copula in tomography in the case of only two projections. The original 1 image simulated is a Gaussian and the original 2 image is formed by four Gaussians. We performed BP, FBP, MBP and CopBP on these images. We observe the MBP and the CopBP, the two projections on the reconstructed images match those from the simulated images which are not the cases for the BP and the FBP.

7. Conclusion

The main contribution of this paper is to find a link between the notion of *copulas* in statistics and X-ray CT for small number of projections. This link brings up possible new approaches for image reconstruction in CT. We first presented the bivariate copulas and the image reconstruction problem in CT. We highlight the connexion between the two problems that consist in i) determining a joint bivariate pdf from its two marginals and ii) the CT image reconstruction from only two horizontal and vertical projections.

We emphasize that in both cases, we have the same inverse problem for the determination of a bivariate function (an image) from the line integrals. We have indicated the potential of copula-based reconstruction methods, introducing the MBP (Multiplicative Back Projection) and CopBP (Copula Back Projection) methods. Current work addresses the characterization of family of copulas as well as the estimation of copulas parameters in the reconstruction process. We also intend to improve the results by accounting for more projections in the method, while keeping the copula approach.

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